

Review Problem Set - MRI

1. Consider a 1.5T magnet with $G_z=20$ mT/m, the difference in Larmor frequency between the magnet isocenter ($z=0$) and a position $z=1$ cm is equal to,
 - a) 8.52 kHz
 - b) 8.52 MHz
 - c) 63.9 MHz
2. The axes in the rotating frame of reference differ from those in the laboratory frame of reference in that,
 - a) Each of the transverse axes precess about their direction at the Larmor frequency
 - b) The z-axis precesses at the Larmor frequency
 - c) Both x and y axes rotate around the z-axis at the Larmor frequency
3. In order to change the flip angle of the RF pulse,
 - a) Change the bandwidth of the RF pulse
 - b) Change the amplitude of the RF pulse
 - c) Change amplitude of the slice selection gradient
4. In order to change the slice profile,
 - a) Change the envelope of the RF pulse at the same bandwidth
 - b) Change the RF pulse amplitude
 - c) Change the slice selection gradient
5. It is possible to reverse the action of magnetic field inhomogeneity dephasing in FID signals when using,
 - a) Gradient echo sequence
 - b) Spin-echo sequence
 - c) Inversion recovery sequence
6. The signal after a perfect 180 degree RF pulse is expected to be,
 - a) Zero
 - b) T1-weighted
 - c) T2* weighted
7. Comparing a gradient-echo and a spin-echo sequences with the same parameters (TR/TE, flip angle, etc.), the signal from gradient-echo is always,
 - a) Smaller
 - b) Larger
 - c) Equal but opposite in phase
8. To measure T1, we usually use,
 - a) Gradient echo pulse sequence
 - b) Spin echo pulse sequence
 - c) Inversion recovery pulse sequence
9. Magnetic resonance spectroscopy can be used for,
 - a) Mapping concentration of different nuclei in the human body noninvasively
 - b) Mapping concentration of different metabolites in the human body noninvasively
 - c) Mapping magnetic field inhomogeneity in PPM scale inside the magnet
10. The T2-weighted MR image depends on,
 - a) Only T2 values inside the body
 - b) Only spin density inside the body
 - c) Both spin density and T2 inside the body

11. A material that is chemically shifted from water by 1.7kHz has a different resonance frequency at 4T from that of water by approximately,
- 1 ppm.
 - 10 ppm.
 - 100 ppm.
12. To null a tissue with $T_1=300$ ms using inversion recovery, we should use a T_I equal to approximately,
- 200 ms
 - 300 ms
 - 400 ms
13. The net magnetization refers to
- The remaining magnetization after T_2^* decay.
 - The difference between spins pointing with B_0 and those pointing against B_0
 - The magnetization in the transverse plane at equilibrium.
14. As the static magnetic field becomes higher, the MR signal from is expected to,
- Increase quadratically
 - Decrease linearly
 - Increase linearly
15. The tipped magnetization vector under the laboratory frame of reference appears,
- Precessing around z-axis at the Larmor frequency
 - Stationary
 - Rotating at the Larmor frequency.
16. In order to change the slice position of the RF pulse,
- Change the pulse modulation frequency
 - Change the slice selection gradient position
 - Change the position of the patient
17. In order to change the slice thickness,
- Change the slice amplitude
 - Change the envelope at the same bandwidth
 - Change the slice selection gradient
18. The rate at which the measured signal in the transverse plan disappears is a function of,
- T_1
 - T_2
 - T_2^*
19. The rate at which the inverted magnetization in inversion recovery sequences relaxes depends on,
- T_1
 - T_2
 - T_2^*
20. The signal decays fast in free induction decay because of,
- Spin-spin relaxation
 - Spin dephasing
 - Spin lattice relaxation
21. The signal at time TE in a spin echo pulse sequence depends on,
- T_1
 - T_2
 - T_2^*
22. To measure T_1 , we usually use,
- Inversion recovery pulse sequence
 - Gradient echo pulse sequence

- c) Spin echo pulse sequence
23. Magnetic fields in the Tesla range are used for MRI because,
- a) they are easier to generate
 - b) they allow a stronger signal to be obtained
 - b) they provide better T1/T2 values
 - d) the existing magnets happen to be in that range
 - c) they provide lower noise
24. Rotating frame is preferred to lab frame because,
- a) Rotating frame makes it easier to follow the motion of net magnetization
 - b) It provides a nicer polar representation instead of the usual Cartesian form
 - c) It makes it easier to image claustrophobic patients
 - d) It makes it faster to perform imaging
 - e) It reduces motion artifacts
25. Net magnetization can be observed only when,
- a) it is in the rotating frame of reference
 - b) it is in the lab frame
 - b) it is in the equilibrium position
 - d) it is in the transverse plane
 - c) it is in the same direction as B_0 .
26. Equilibrium position of net magnetization can be reached after an RF pulse is followed by a delay that is equal to,
- a) $5 T_2$
 - b) TR
 - c) TE
 - d) $5 T_2^*$
 - e) $5 T_1$
27. To control the slice thickness of an RF pulse, one can do the following:
- a) Change the modulation of the RF pulse
 - b) Change the duration of the RF pulse
 - c) Change the bandwidth of the RF pulse
 - d) Change the amplitude of the RF pulse
 - e) Change the direction of the X and Y RF coils
28. A T_2^* -weighted pulse sequence can be,
- a) A spin-echo sequence with long TR and long TE
 - b) A gradient echo sequence with short TR and short TE
 - c) A spin-echo sequence with short TR and long TE
 - d) A gradient sequence with long TR and long TE
 - e) A spin-echo sequence with long TR and short TE
29. A slice selection gradient of 5 mT/m if combined with an RF pulse of bandwidth of 1kHz will select a slice of thickness:
- a) 1 cm
 - b) 1 mm
 - c) 2 mm
 - d) 5 mm
 - e) 8 mm
30. Aliasing artifact in the phase encoding direction results from:
- a) A number of phase encoding steps that is too small
 - b) A number of phase encoding steps that is too large
 - c) A phase encoding step that is too small
 - d) A phase encoding step that is too large
 - e) Under-sampling the received time-domain echoes

31. In designing an RF pulse to select a 5mm slice in a 1.5T magnet, if the slice selection gradient is set at 5mT/m and the desired flip angle is $\pi/6$, a proper design for the duration of a rectangular RF pulse can be selected approximately as:
- 1 msec
 - 2 msec
 - 8 nsec
 - 1 nsec
 - Other:
32. To acquire an oblique slice that makes an angle of 45 degrees with x-, y- and z-axes, the slice selection design consists of:
- Three similar RF pulses in x-, y -, and z-directions with no gradients
 - One RF pulse and no gradients
 - Two RF pulses in x- and y-directions and a gradient in z-direction
 - One RF pulse and equal gradients in x-, y-, and z-directions (*)
 - Other:
33. To control the flip angle of an RF pulse, one can do the following:
- Change the modulation of the RF pulse
 - Change the duration of the RF pulse
 - Change the bandwidth of the RF pulse
 - Change the amplitude of the RF pulse
 - Change the direction of the X and Y RF coils
34. Fourier encoding means:
- Frequency encoding
 - Phase encoding
 - Slice selection
 - Frequency or phase encoding
 - Frequency encoding, phase encoding and slice selection
35. The Larmor frequency at 10 cm away from the iso-center of a 1.5 Tesla magnet is:
- 63.9 MHz
 - 42.6 MHz
 - 28.4 MHz
 - 21.3 MHz
 - 85.2 MHz
36. Frequency encoding can be applied for:
- Spatial encoding in one dimension
 - Spatial encoding in two dimensions
 - Spatial encoding in three dimensions
 - Shimming the magnet
 - Slice selection
37. In conventional gradient echo, a single row in the k-space is filled within each:
- Scan time
 - TE period
 - TR period
 - RF Excitation
 - TI period
38. The field of view is primarily determined by:
- The sampling bandwidth and read-out gradient
 - SNR
 - The number of acquired k-space samples
 - The size of the reception coils

- e) The image resolution.
39. Increasing the voxel size in the phase encoding direction at same coverage will:
- a) Increase the scan time
 - b) Decrease the scan time
 - c) Have no effect on the scan time
 - d) Cause aliasing
 - e) Cause motion artifacts
40. In Fourier imaging sequence, each TR enables the acquisition of:
- a) One point in the image
 - b) One line in the image
 - c) One point in the k-space of the image
 - d) One line in the k-space of the image
 - e) A collection of random points in the image
41. The cause of aliasing artifact is:
- a) The absence of sampling in RO direction
 - b) The absence of sampling in PE direction
 - c) The under-sampling in PE direction
 - d) The over-sampling of the RO direction
 - e) The over-sampling of both the PE and RO directions
42. Cross-talk is the result of:
- a) Interference in signal lines
 - b) Interference between gradient coils
 - c) Overlapping between adjacent slice profiles
 - d) Overlapping of gradients
 - e) Overlapping of RF pulses
43. A slice selection gradient of 5 mT/m if combined with an RF pulse of bandwidth of 1kHz will select a slice of thickness:
- a) 1 cm
 - b) 1 mm
 - c) 2 mm
 - d) 5 mm
 - e) 8 mm
44. The negative gradient lobe applied right before the RO gradient in the same direction is used to:
- a) Make phase encoding
 - b) Make better slice selection
 - c) Allow longer acquisition
 - d) Make center of k-space in the center of acquisition window
 - e) Center image
45. To increase the resolution in the frequency encoding direction for the same FOV,
- a) use higher sampling rate for same duration
 - b) use same sampling rate for longer duration
 - c) use higher sampling for longer duration
 - d) apply additional phase encoding
 - e) use a thinner slice selection
46. The key component for spatial encoding in MRI systems is,
- a) main magnet
 - b) quadrature coils
 - c) gradient coils

- d) shim coils
 - e) gantry
47. In a multi-slice TOF MRA imaging sequence, the scan parameters were: TR/TE: 300/20 msec, FOV: 20cm x 20cm, Matrix 256x256, Number of slices: 128, slice thickness: 5mm, NEX: 2, flip angle: 30 degrees. The shortest total acquisition time for this sequence is approximately:
- a) 18 minutes
 - b) 245 minutes
 - c) 2 minutes
 - d) 9 minutes
 - e) Other:
48. Image resolution can be expressed in units of,
- a) bits
 - b) lp/mm
 - c) 1/sec
 - d) mm/sec
 - e) points
49. Inversion time for suppressing fat ($T_1=300$ ms) in an image is approximately,
- a) 400 ms
 - b) 800 ms
 - c) 200 ms
 - d) 1 sec
 - e) other:
50. The resolution in the read-out direction depends on,
- a) Sampling duration (k-space coverage)
 - b) Sampling bandwidth (k-space sampling rate)
 - c) Sampling dynamic range (number of bits of sampling A/D)
51. The FOV in the phase encoding direction depends mainly on,
- a) Phase encoding step size only
 - b) Number of phase encoding steps and step size
 - c) Matrix size in the phase encoding direction only
52. To maintain the same resolution in the read-out direction at a larger FOV, one can,
- a) Increase the k-space sampling bandwidth only
 - b) Increase the k-space coverage in the read-out direction only
 - c) Increase both k-space sampling bandwidth and k-space coverage
53. The acquisition time for 30 128x128 slices when NEX=2, TE=50 ms, and TR=1 sec is approximately,
- a) 8.5 min
 - b) 4.3 min
 - c) 6.4 min
54. For a multi-slice imaging sequence with parameters given as: slice thickness: 5mm, flip angle: 60 degrees, matrix size: 128x192, FOV: 20cmx25cm, NEX: 1, and TR/TE: 600/20, the ratio of acquisition time to acquire 25 slices to that of acquiring 20 slices using this sequence is,
- a) 1
 - b) 1.25
 - c) 2
55. A material that is chemically shifted from water by 1.7k has a different resonance frequency at 4T from that of water by approximately,
- a) 10 ppm.
 - b) 100 ppm.

- c) 1 ppm.
56. The total acquisition time for a 3-D Fourier acquisition of a volume of matrix size $128 \times 128 \times 256$ with TR/TE: 100/15ms is approximately,
- 14 minutes.
 - 27 minutes.
 - 54 minutes.
57. The k-space represents,
- The Fourier domain of the image
 - The MR image space
 - The space where k-space trajectories are designed.
58. The FOV in the read-out direction depends on,
- Sampling bandwidth
 - Sampling duration
 - Sampling dynamic range
59. The FOV in the phase encoding direction depends mainly on,
- Phase encoding step size
 - Number of phase encoding steps
 - Matrix size in the phase encoding direction
60. The implementation of FOV selection in MRI systems is done through,
- Proper selection of sampling steps in k_x and k_y directions.
 - Proper selection of k-space coverage in k_x and k_y directions.
 - Proper positioning of the patient inside the magnet.
 - Proper adjustment of the image reconstruction software.
 - Proper selection of the Larmor frequencies inside the patient.
61. Given a 60 degrees RF pulse that is implemented using a Sinc time domain envelope using a slice selection gradient $G_z=15\text{mT/m}$ at 1.5T to excite a 3mm slice centered at $z=1\text{cm}$, we can derive another RF pulse to excite a similar slice profile at $z=2\text{cm}$ by modifying the current pulse as follows,
- Increase the modulation frequency by 6.4kHz.
 - Shift the slice selection gradient by 1 cm.
 - Double the time domain width of the RF pulse.
 - Decrease the amplitude of the RF pulse by one half.
 - Change the RF envelope function.
62. Draw a properly labeled T2-weighted magnetic resonance imaging sequence that can be used for imaging 3-D volume using 3 -D Fourier imaging. Draw a clear diagram of its k-space trajectory.
63. Draw a properly labeled T2* -weighted sequence that has the shown k-space trajectory:

