



# **Medical Image Reconstruction**

## **Term II - 2012**

### **Topic 6:**

# **Tomography**

Professor Yasser Mostafa Kadah

# Tomography

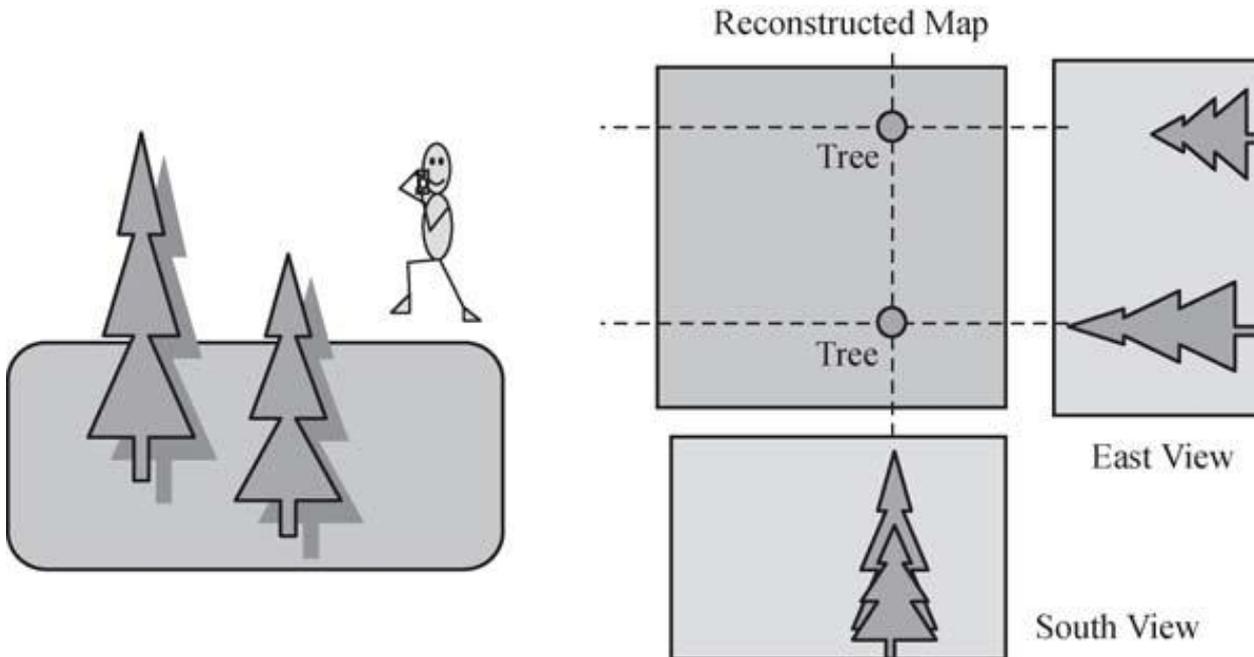
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- ▶ The Greek word “*tomos*” means a section, a slice, or a cut.
- ▶ Tomography is the process of imaging a cross section
- ▶ Particularly useful in medical imaging
  - ▶ Nobody wants to be cut open to see what is inside!



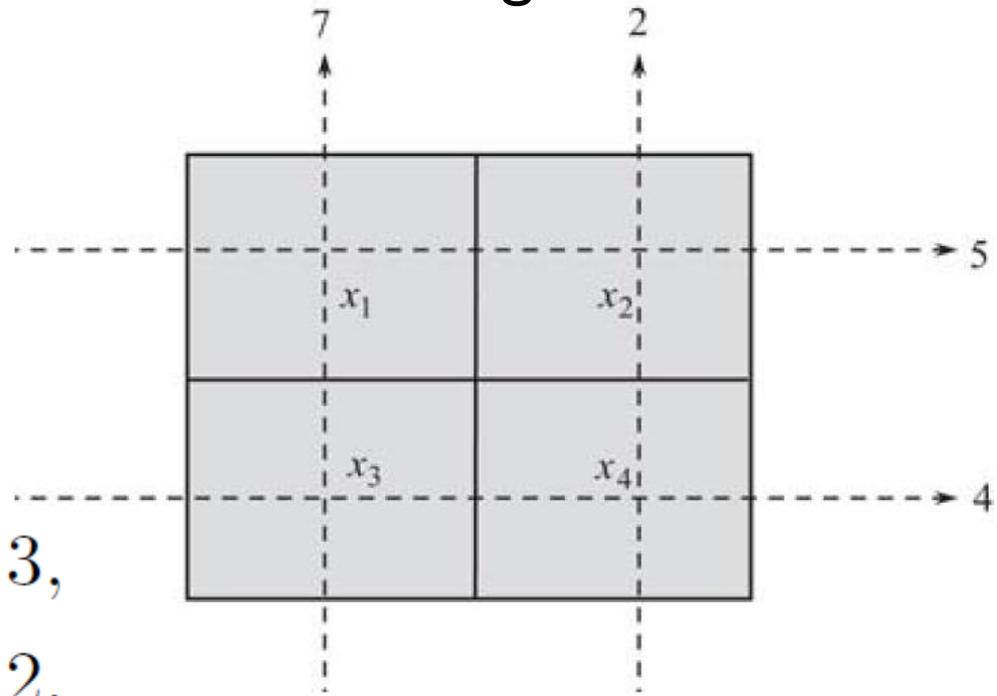
# Example

- ▶ Can you compute the locations of the trees from 2 images?
  - ▶ Answer: Yes



# Example

- ▶ Can you compute the values of this matrix given its projections?
  - ▶ Answer: Yes



$$x_1 + x_2 = 5,$$

$$x_3 + x_4 = 4,$$

$$x_1 + x_3 = 7,$$

$$x_2 + x_4 = 2.$$

$$x_1 = 3,$$

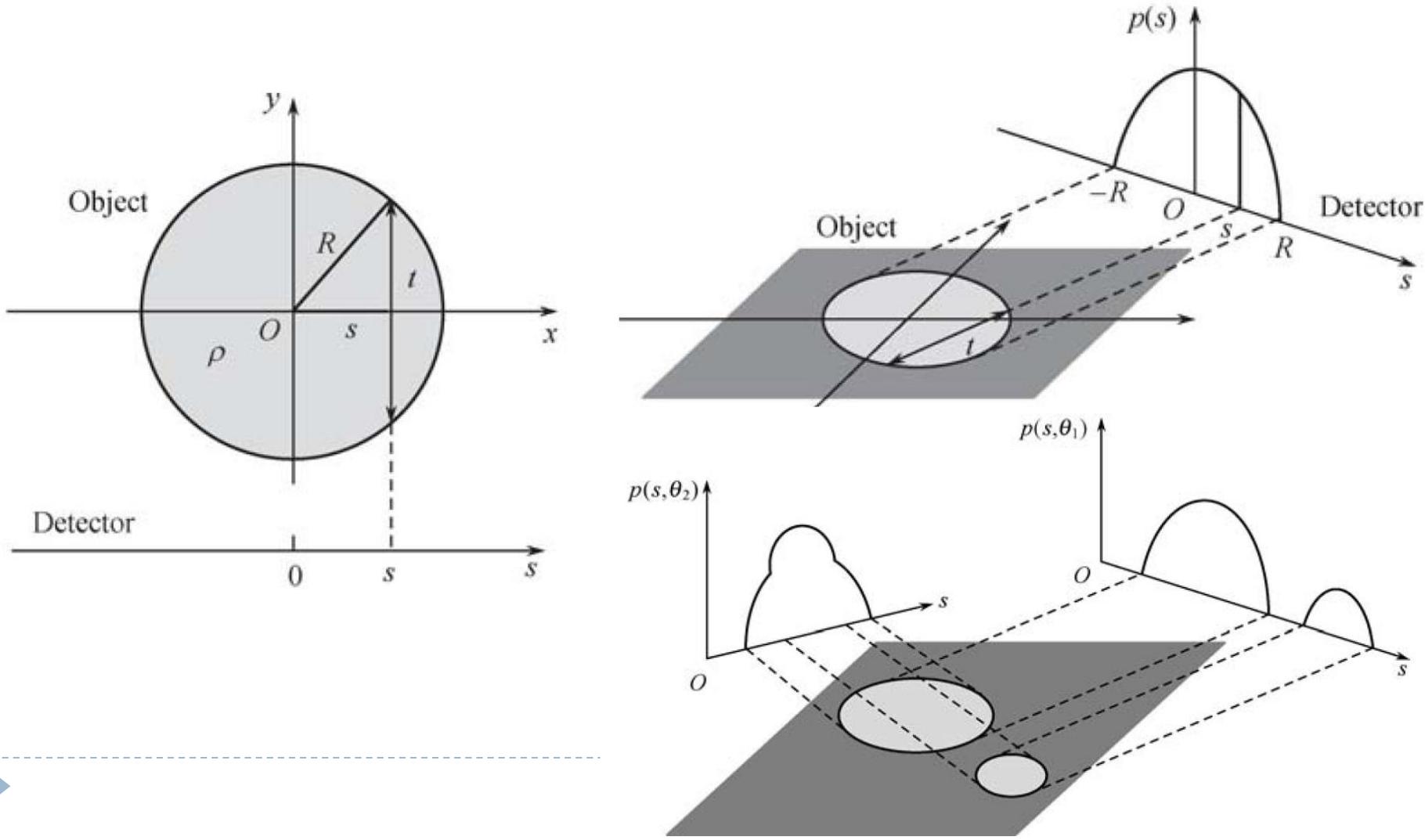
$$x_2 = 2,$$

$$x_3 = 4,$$

$$x_4 = 0.$$

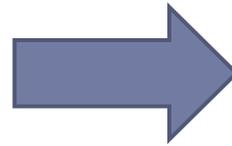
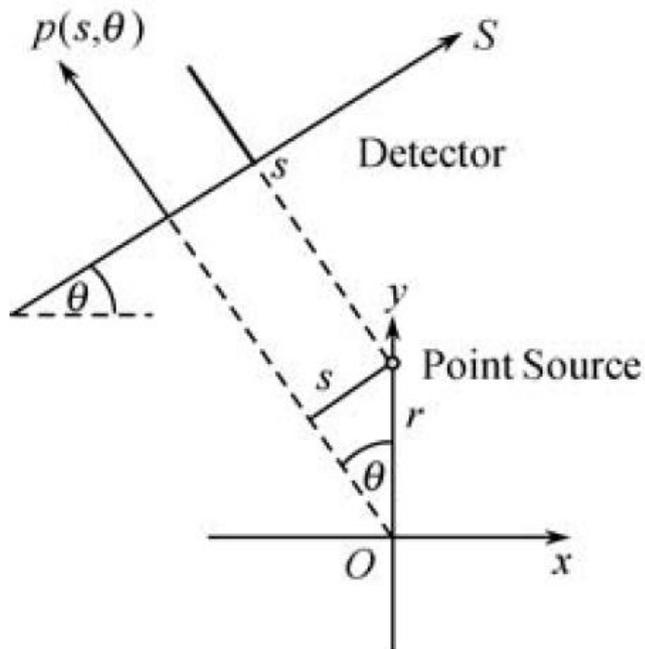
# Projection

- ▶ Also termed *ray sum*, *line integral*, or *Radon transform*

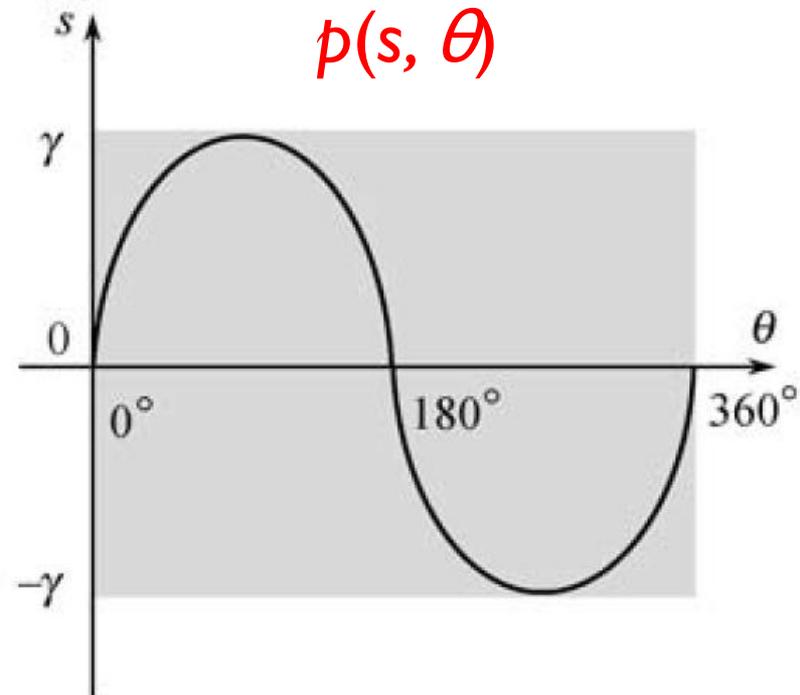


# Sinogram

- ▶ Displays angle dependence of projections
  - ▶ Example: point source on the  $y$ -axis to further illustrate the angle  $\theta$  dependency of the projection  $p(s, \theta)$

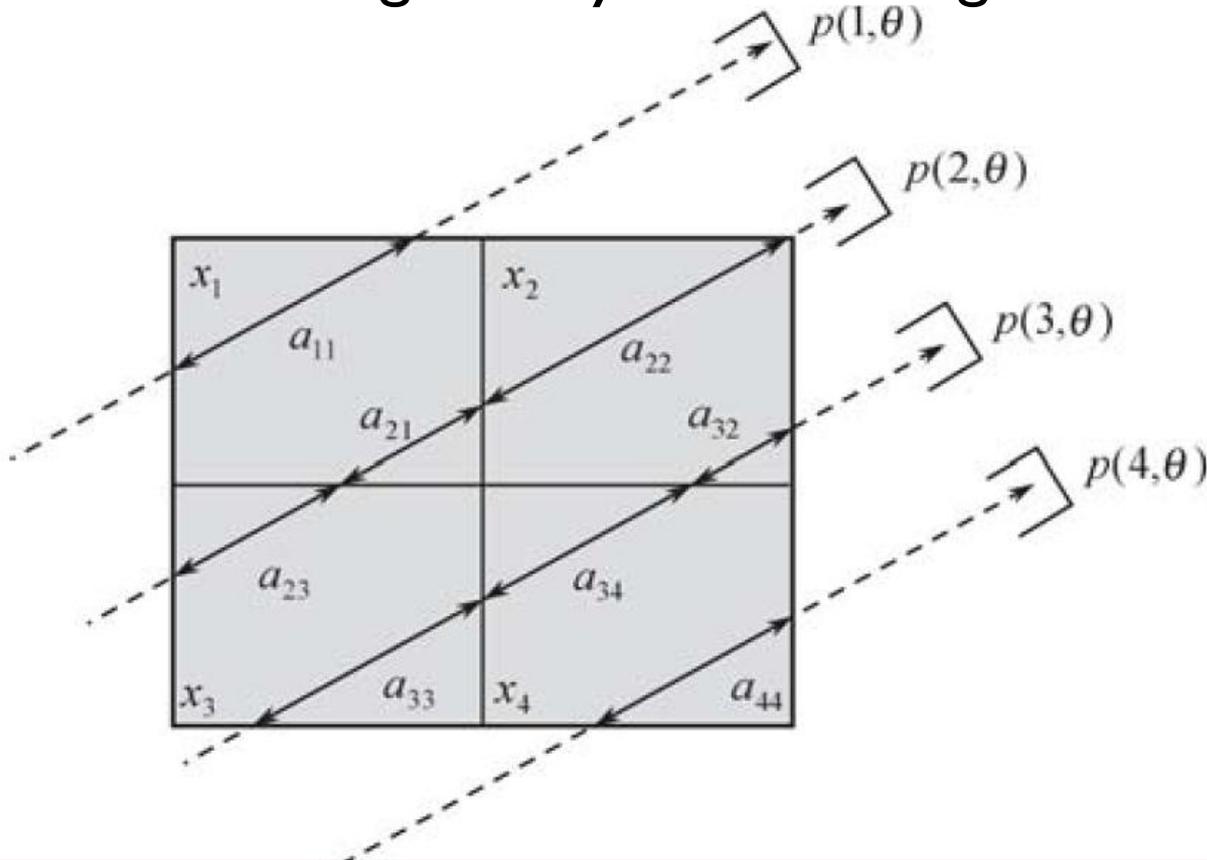


## Sinogram $p(s, \theta)$



# Projection of Discrete Object

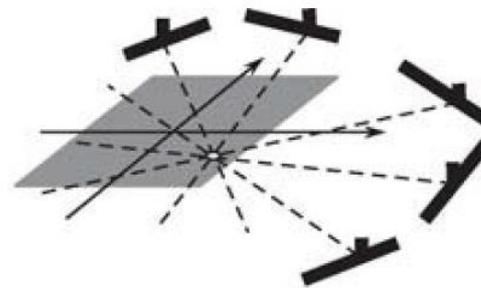
- ▶ Projections are weighted by the line-length within each pixel



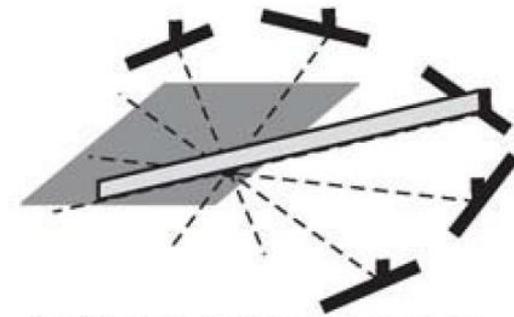
$$p(i, \theta) = a_{i1}x_1 + a_{i2}x_2 + a_{i3}x_3 + a_{i4}x_4, \quad i = 1, 2, 3, 4.$$

# Image Reconstruction of a Point Source

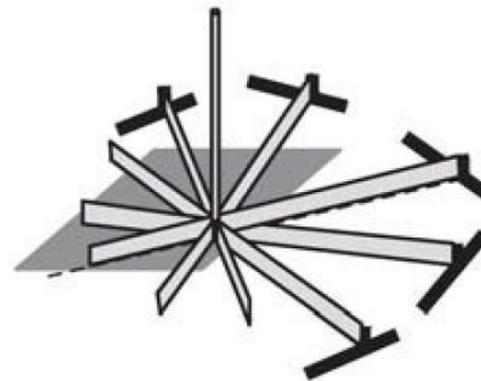
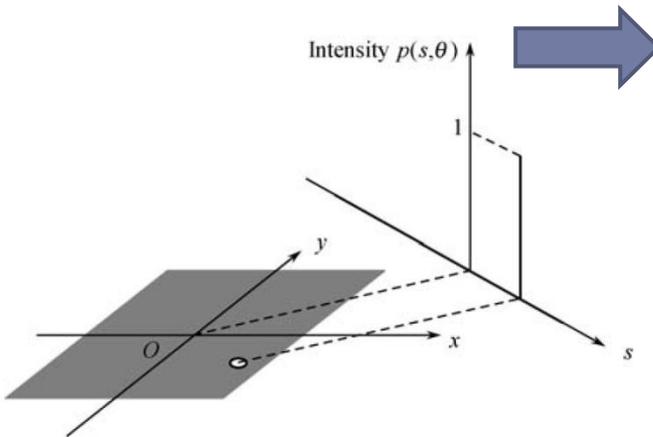
- ▶ In image reconstruction, we not only need to find the location but also the intensity value of the object of interest
  - ▶ Backprojection



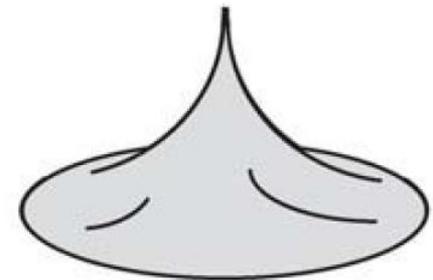
(a) Project a point source



(b) Backproject from one view



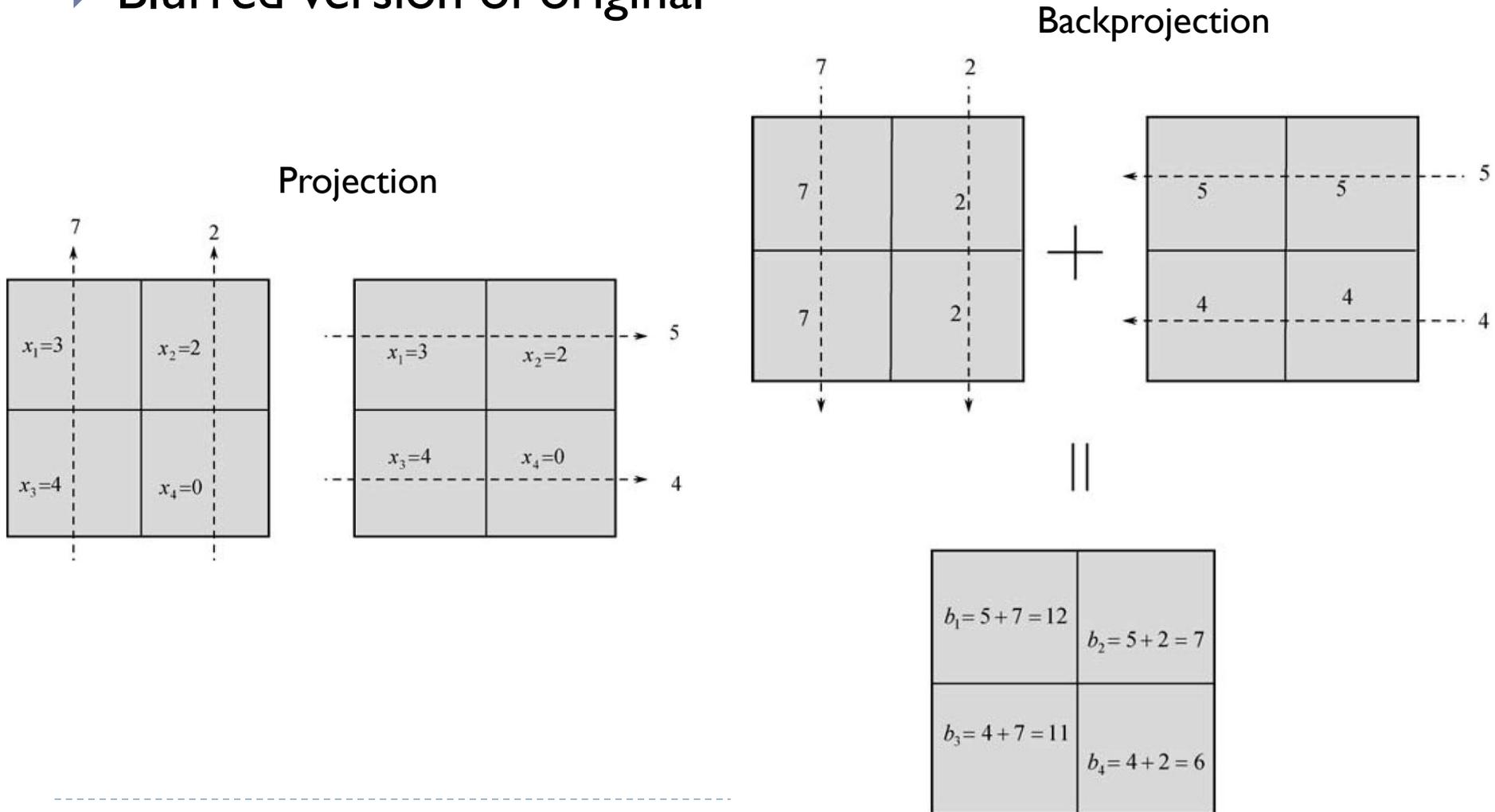
(c) Backproject from a few views



(d) Backproject from all views

# Backprojection Example

- ▶ Blurred version of original

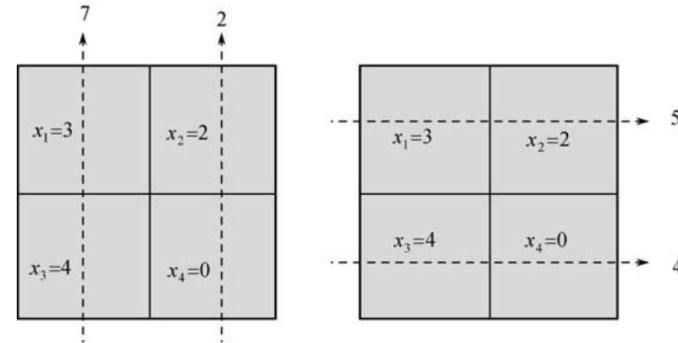


# Backprojection in Algebraic Form

## ► Projection P

$$P = AX, \quad X = [x_1, x_2, x_3, x_4]^T$$

$$A = \begin{bmatrix} 1 & 0 & 1 & 0 \\ 0 & 1 & 0 & 1 \\ 1 & 1 & 0 & 0 \\ 0 & 0 & 1 & 1 \end{bmatrix}$$



$$P = [p(1, 0^\circ), p(2, 0^\circ), p(1, 270^\circ), p(2, 270^\circ)]^T = [7, 2, 5, 4]^T.$$

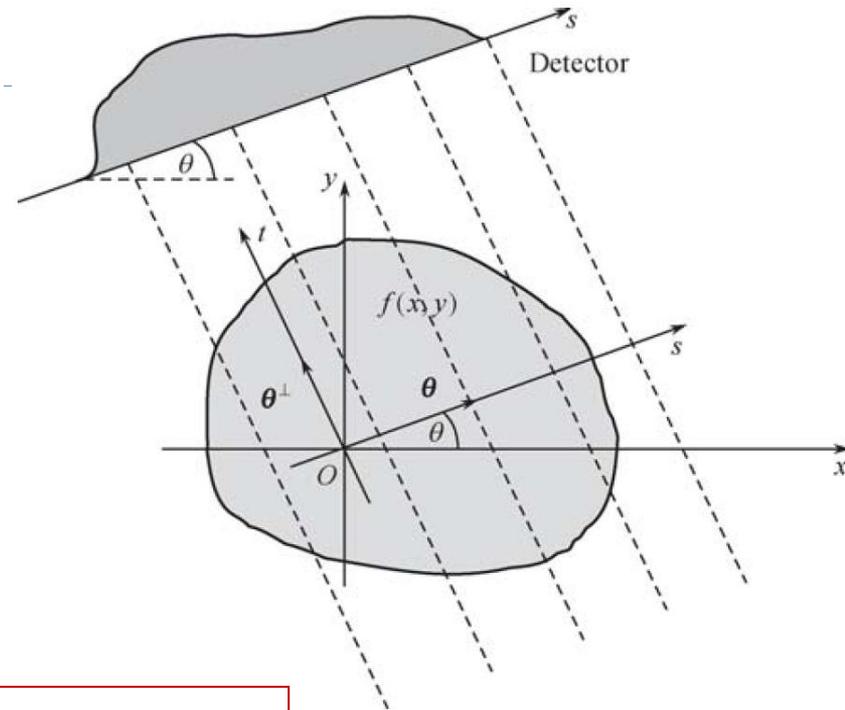
## ► Backprojection: use adjoint operator $A^T$

$$B = A^T P = \begin{bmatrix} 1 & 0 & 1 & 0 \\ 0 & 1 & 0 & 1 \\ 1 & 1 & 0 & 0 \\ 0 & 0 & 1 & 1 \end{bmatrix}^T \begin{bmatrix} 7 \\ 2 \\ 5 \\ 4 \end{bmatrix} = \begin{bmatrix} 1 & 0 & 1 & 0 \\ 0 & 1 & 1 & 0 \\ 1 & 0 & 0 & 1 \\ 0 & 1 & 0 & 1 \end{bmatrix} \begin{bmatrix} 7 \\ 2 \\ 5 \\ 4 \end{bmatrix} = \begin{bmatrix} 12 \\ 7 \\ 11 \\ 6 \end{bmatrix}$$

# Radon Transform

- ▶ Computes parallel projections at specific angles

$$f(x,y) \rightarrow p(s,\theta)$$



$$p(s,\theta) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} f(x,y) \delta(x \cos \theta + y \sin \theta - s) dx dy,$$

$$p(s,\theta) = \int_{-\infty}^{\infty} f(s \cos \theta - t \sin \theta, s \sin \theta + t \cos \theta) dt,$$

$$\mathcal{R}f(t,\theta) := \int_{l_{t,\theta}} f ds = \int_{s=-\infty}^{\infty} f(t \cos(\theta) - s \sin(\theta), t \sin(\theta) + s \cos(\theta)) ds.$$

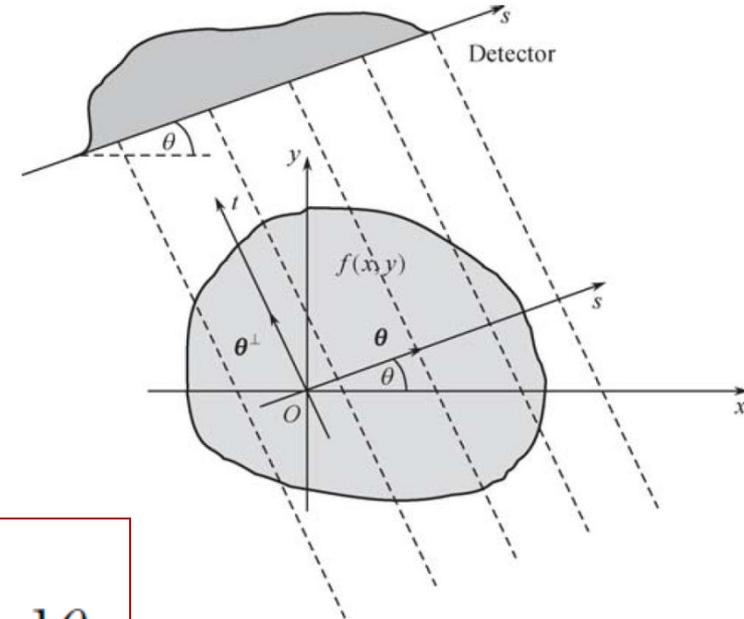
# Inverse Radon Transform

## ▶ Parallel Beam Backprojection

$$p(s, \theta) \rightarrow f(x, y)$$

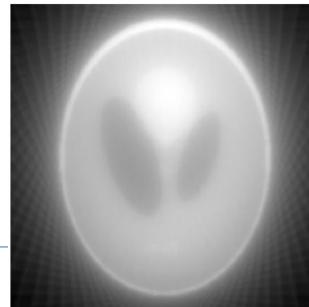
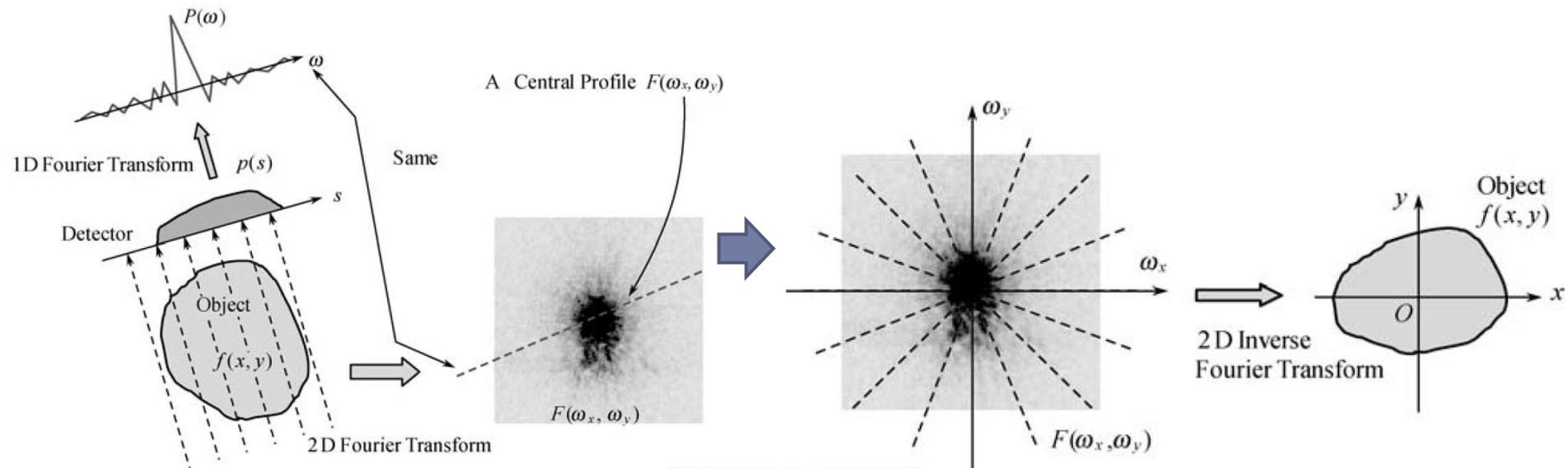
$$b(x, y) = \int_0^\pi p(s, \theta) \Big|_{s=x \cos \theta + y \sin \theta} d\theta,$$

$$b(x, y) = \int_0^\pi p(\mathbf{x} \cdot \boldsymbol{\theta}, \theta) d\theta,$$



# Backprojection in Frequency Domain

- ▶ Each view adds a line in the Fourier space
  - ▶ Central area in k-space has higher sample density and results in effective lowpass filtered spectrum



# Filtered Backprojection

- ▶ To counter this blurring effect, we must compensate for the non-uniformity in the Fourier space

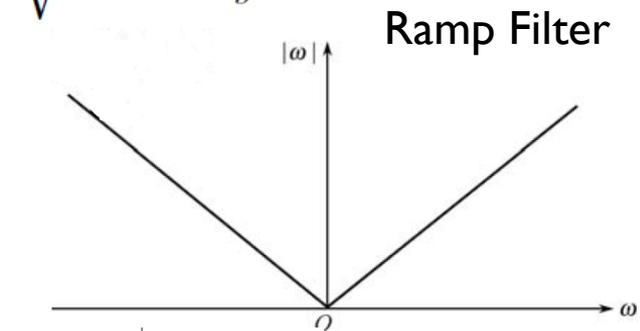
- ▶ Density in the Fourier space is proportional to:  $\frac{1}{\sqrt{\omega_x^2 + \omega_y^2}}$ .

- ▶ Solution: multiply k-space by ramp filter;

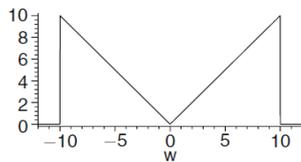
$$\sqrt{\omega_x^2 + \omega_y^2}$$

- ▶ Method 1: Filter individual projections
- ▶ Method 2: Filter whole Image

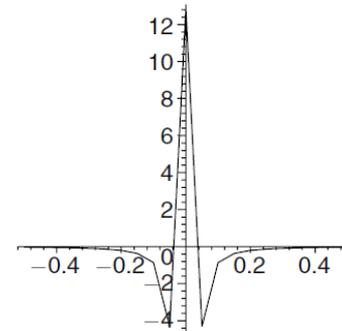
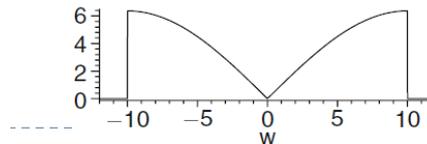
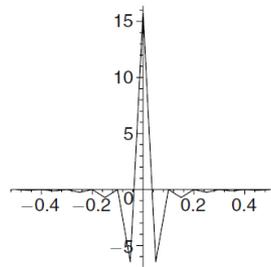
- ▶ Practical Realization



Ram-Lak Filter



Shepp-Logan Filter



# Hilbert Transform Based Formulation

$$\mathcal{F} \left( \frac{df}{dx} \right) (\omega) = i\omega \mathcal{F}(f)(\omega). \quad \rightarrow \quad \mathcal{F} \left( \frac{\partial(\mathcal{R}f)(t, \theta)}{\partial t} \right) (S, \theta) = iS \mathcal{F}(\mathcal{R}f)(S, \theta).$$

$$|S| = S \cdot \text{sgn}(S)$$

$$i \cdot \text{sgn}(S) \cdot \mathcal{F} \left( \frac{\partial(\mathcal{R}f)(t, \theta)}{\partial t} \right) (S, \theta) = -|S| \mathcal{F}(\mathcal{R}f)(S, \theta).$$

$$f(x, y) = \frac{-1}{2} \mathcal{B} \left\{ \mathcal{F}^{-1} \left[ i \cdot \text{sgn}(S) \cdot \mathcal{F} \left( \frac{\partial(\mathcal{R}f)(t, \theta)}{\partial t} \right) (S, \theta) \right] \right\} (x, y).$$

Define Hilbert Transform as:  $\mathcal{H} g(t) = \mathcal{F}^{-1} [i \cdot \text{sgn}(\omega) \cdot \mathcal{F} g(\omega)] (t).$

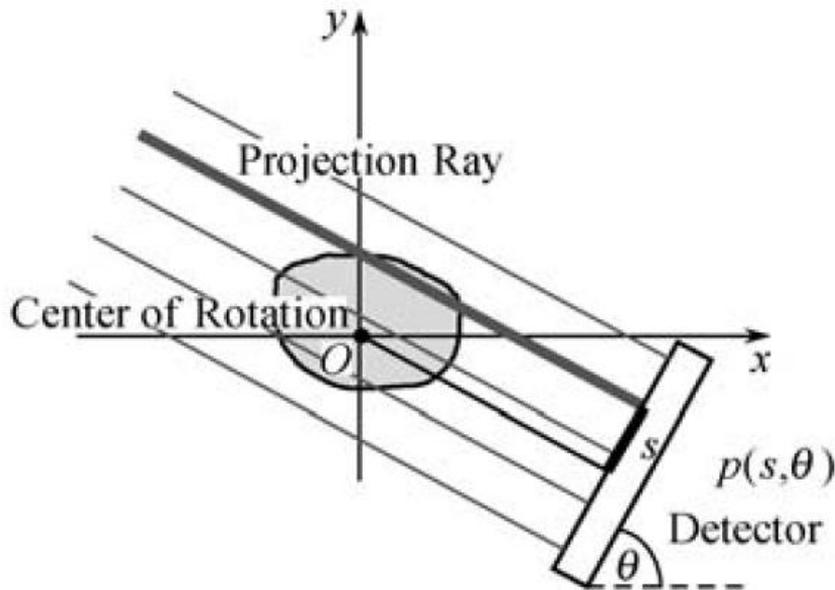
$$\rightarrow f(x, y) = \frac{-1}{2} \mathcal{B} \left[ \mathcal{H} \left( \frac{\partial(\mathcal{R}f)(t, \theta)}{\partial t} \right) (S, \theta) \right] (x, y).$$

# Parallel Beam Reconstruction Methods

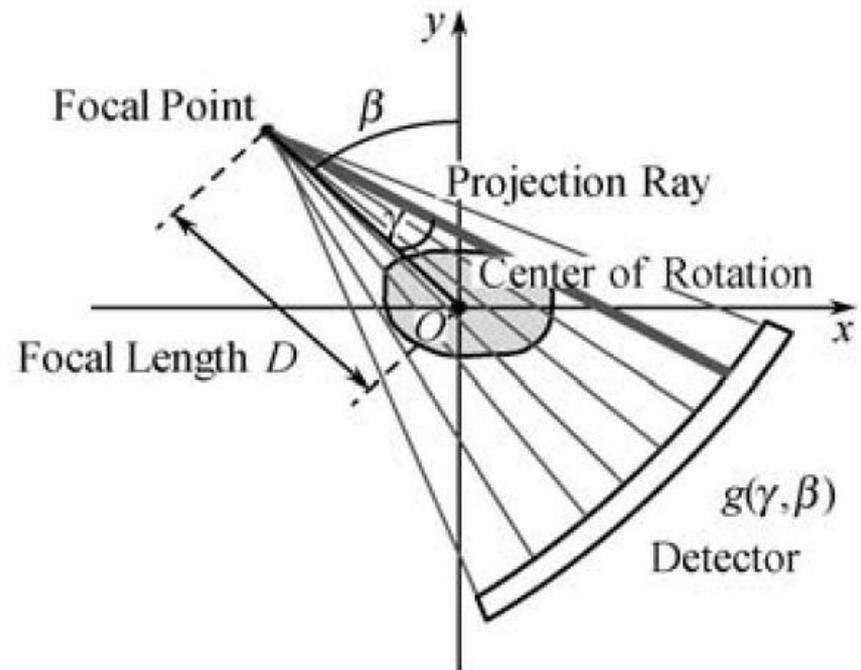
Method	Step 1	Step 2	Step 3
1	1D Ramp filter with Fourier transform	Backprojection	---
2	1D Ramp filter with convolution	Backprojection	
4	Backprojection	2D Ramp filter with Fourier transform	
	Backprojection	2D Ramp filter with 2D convolution	
3	Derivative	Hilbert transform	Backprojection
5	Derivative	Backprojection	Hilbert transform
	Backprojection	Derivative	Hilbert transform
	Hilbert transform	Derivative	Backprojection
	Hilbert transform	Backprojection	Derivative
	Backprojection	Hilbert transform	Derivative

# Fan Beam Reconstruction Problem

- ▶ Almost all present CT systems use fan beam rather than parallel beam projections
  - ▶ Much more efficient: faster acquisition, lower patient dose



(a) Parallel Beam

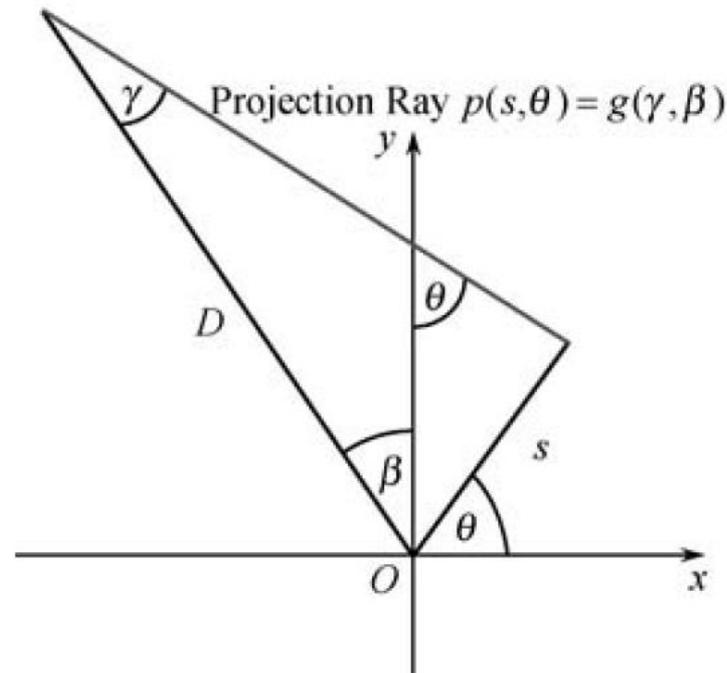


(b) Fan Beam

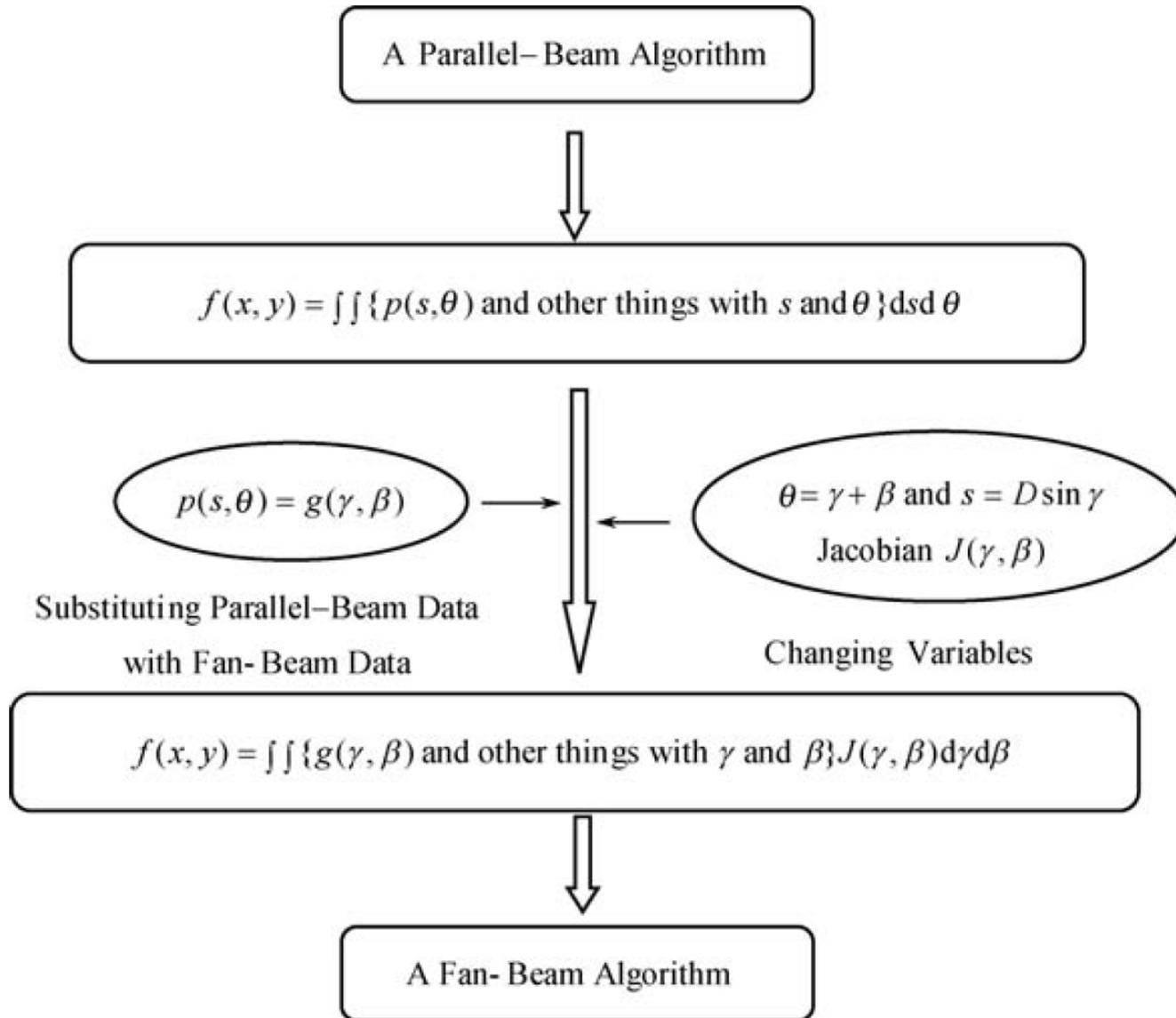
# Fan Beam Reconstruction Problem

- ▶ rebin every fan-beam ray into a parallel-beam ray. For each fan-beam ray-sum  $g(\gamma, \beta)$ , we can find a parallel beam ray-sum  $p(s, \theta)$  that has same orientation as the fan-beam ray with the relations,

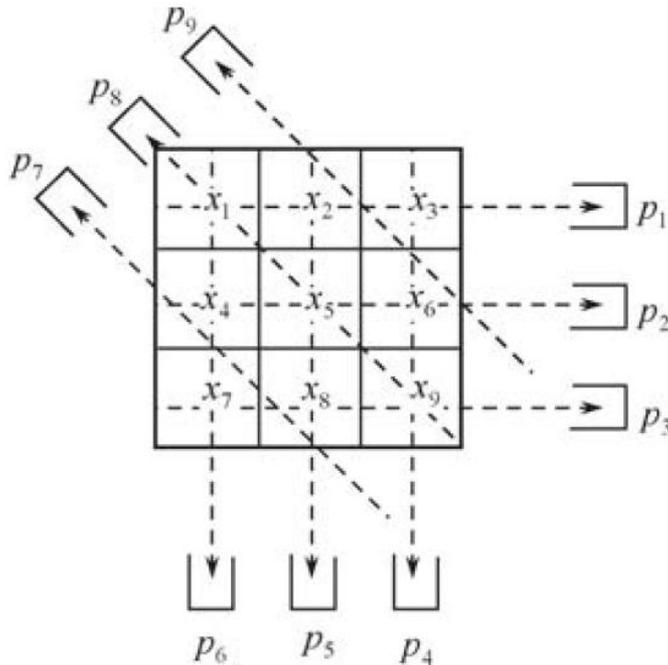
$$\theta = \gamma + \beta, \quad s = D \sin \gamma, \quad \Rightarrow \quad p(s, \theta) = g(\gamma, \beta).$$



# Fan Beam Reconstruction Problem



# Algebraic Reconstruction Technique



$$\begin{cases} x_1 + x_2 + x_3 = p_1, \\ x_4 + x_5 + x_6 = p_2, \\ x_7 + x_8 + x_9 = p_3, \\ x_3 + x_6 + x_9 = p_4, \\ x_2 + x_5 + x_8 = p_5, \\ x_1 + x_4 + x_7 = p_6, \\ 2(\sqrt{2} - 1)x_4 + (2 - \sqrt{2})x_7 + 2(\sqrt{2} - 1)x_8 = p_7, \\ \sqrt{2}x_1 + \sqrt{2}x_5 + \sqrt{2}x_9 = p_8, \\ 2(\sqrt{2} - 1)x_2 + (2 - \sqrt{2})x_3 + 2(\sqrt{2} - 1)x_6 = p_9. \end{cases}$$

$$AX = P,$$

$$X = A^+ P = V \Sigma^+ U^T P.$$

$$\mathbf{x}^{next}$$

$$= \mathbf{x}^{current} - \text{Backproject}_{ray} \left\{ \frac{\text{Project}_{ray}(\mathbf{x}^{current}) - \text{Measurement}_{ray}}{\text{Normalization Factor}} \right\}.$$

# Other Algebraic Methods

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- ▶ Gradient descent

$$\mathbf{x}^{next} = \mathbf{x}^{current} - a_{current} \Delta(\mathbf{x}^{current}),$$

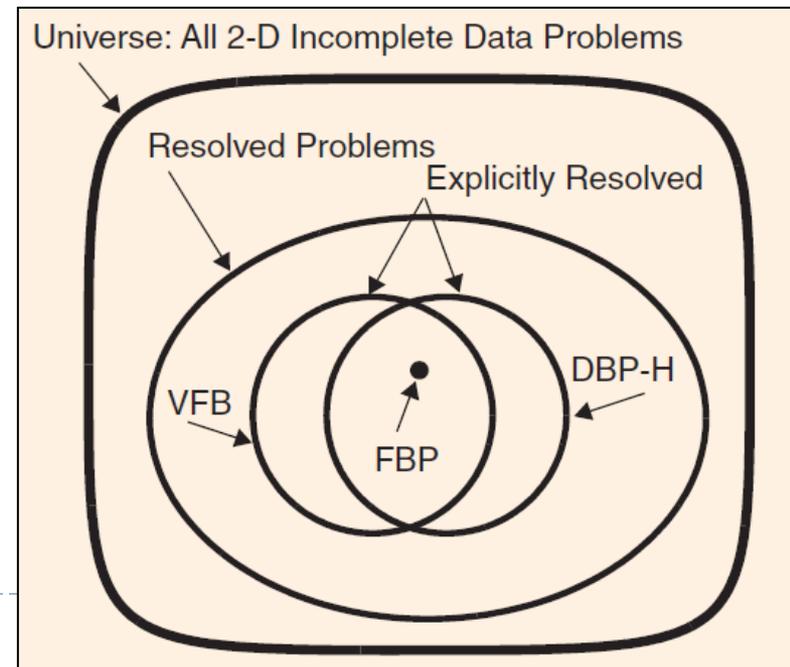
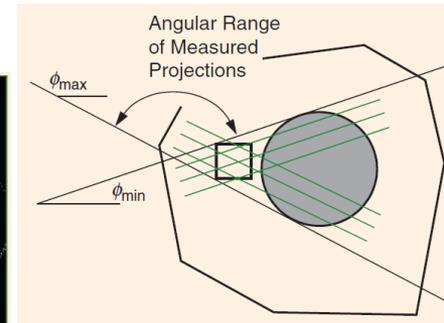
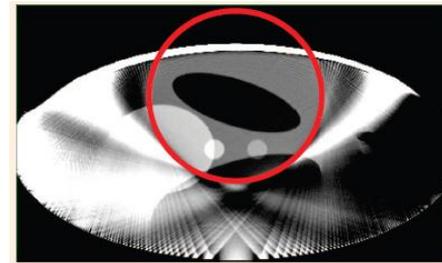
- ▶ Maximum-Likelihood Expectation-Maximization

$$\mathbf{x}^{next} = \mathbf{x}^{current} \frac{\text{Backproject} \left\{ \frac{\text{Measurement}}{\text{Project}(\mathbf{x}^{current})} \right\}}{\text{Backproject} \{ \mathbf{1} \}},$$



# Advanced Tomography Problems

- ▶ Reconstruction from incomplete data
  - ▶ Truncated projections
  - ▶ Limited-angle projections
  - ▶ Exterior data
  - ▶ ROI reconstruction
- ▶ Extension to 3D
- ▶ Stability of reconstruction



# Matlab Functions

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- ▶ Look up the help for the following function:
  - ▶ radon
  - ▶ iradon
  - ▶ fan2para
  - ▶ fanbeam
  - ▶ ifanbeam
  - ▶ para2fan
  - ▶ phantom



# Exercise

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- ▶ P1. For a medical image of your choice:
    - ▶ A. Generate the Radon transform and display its sinogram
    - ▶ B. Reconstruct the image back from its projections
    - ▶ C. Compare the two images and record the error for different numbers of projections and provide your comments.
  - ▶ P2. Repeat the above problem P1 for a fan beam system (rather than the parallel beam system in P1). Also, compare the parallel beams obtained from rebinning the fan rays and comment on what you found.
  - ▶ P3. Compare different filtering strategies and provide your choice of the best methodology based on an experimental study. (study filter type and support, 1D vs. 2D implementation, etc.)
  - ▶ P4. Compare the parallel beam projections obtained from a Shepp-Logan phantom to the ones you generate using the analytical Shepp-Logan phantom and comment on the results.
  - ▶ P5. Do a literature review on ONE advanced tomography problem and come up with a 1 page summary of the state of the art and a comprehensive list of references.
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